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(54) **SYSTEMS AND METHODS FOR TREATMENT OF SLEEP APNEA**

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(52) **U.S. Cl.**

CPC ... **A61F 5/56** (2013.01); **A61F 2/00** (2013.01);
A61F 5/566 (2013.01); **A61F 2210/0004** (2013.01)

(58) **Field of Classification Search**

CPC combination set(s) only.
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,424,208	A	1/1984	Wallace et al.
4,582,640	A	4/1986	Smestad et al.
4,978,323	A	12/1990	Freedman
5,041,138	A	8/1991	Vacanti et al.
5,145,935	A	9/1992	Hayashi

(Continued)

FOREIGN PATENT DOCUMENTS

EP	1216013	B1	6/2006
EP	2561842	A1	2/2013

(Continued)

OTHER PUBLICATIONS

Gillis et al.; U.S. Appl. No. 14/275,426 entitled "System and methods for treatment of sleep apnea," filed May 12, 2014.

(Continued)

Primary Examiner — Ophelia A Hawthorne

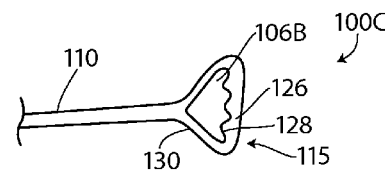
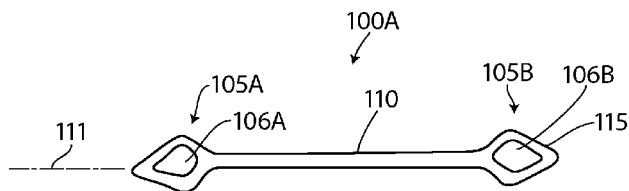
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(57)

ABSTRACT

A system for revisably treating an airway disorder is provided with an implant body configured to conform to an airway-interface tissue site in a manner compatible with normal physiological function of the site. In some embodiments, first and second openings extend through first and second implant ends, respectively, for permitting a tissue plug to grow through each opening. Methods of using and revising such systems are also provided.

22 Claims, 13 Drawing Sheets



(56)

References Cited

U.S. PATENT DOCUMENTS

5,326,355	A	7/1994	Landi	8,327,854	B2	12/2012	Gillis et al.
5,372,600	A	12/1994	Beyar et al.	8,409,296	B2	4/2013	Knize et al.
5,428,024	A	6/1995	Chu et al.	8,523,760	B2	9/2013	Gillis
5,506,300	A	4/1996	Ward et al.	8,528,564	B2	9/2013	Paraschac et al.
5,531,761	A	7/1996	Yoon	8,707,960	B2	4/2014	Gillis et al.
5,665,822	A	9/1997	Bitler et al.	8,733,363	B2	5/2014	Gillis et al.
5,697,779	A	12/1997	Sachdeva et al.	8,747,296	B2	6/2014	Gillis
5,762,599	A	6/1998	Sohn	8,776,799	B2	7/2014	Gillis et al.
5,775,322	A	7/1998	Silverstein et al.	9,050,176	B2	6/2015	Datta et al.
5,782,636	A	7/1998	Armstrong et al.	2001/0051815	A1	12/2001	Esplin
5,972,000	A	10/1999	Beyar et al.	2002/0020417	A1	2/2002	Nikolchev et al.
5,972,111	A	10/1999	Anderson	2002/0116050	A1	8/2002	Kocur
5,979,456	A	11/1999	Magovern	2002/0116070	A1	8/2002	Amara et al.
5,988,171	A	11/1999	Sohn et al.	2003/0149445	A1	8/2003	Knudson et al.
6,019,779	A	2/2000	Thorud et al.	2004/0045556	A1	3/2004	Nelson et al.
6,161,541	A	12/2000	Woodson	2004/0139975	A1	7/2004	Nelson et al.
6,165,486	A	12/2000	Marra et al.	2004/0204734	A1	10/2004	Wagner et al.
6,197,043	B1 *	3/2001	Davidson	2005/0004417	A1	1/2005	Nelson et al.
		 A61L 17/04	2005/0065615	A1	3/2005	Krueger et al.
			424/443	2005/0090861	A1	4/2005	Porter
6,231,605	B1	5/2001	Ku	2005/0092332	A1	5/2005	Conrad et al.
6,250,307	B1	6/2001	Conrad et al.	2005/0115572	A1	6/2005	Brooks et al.
6,388,043	B1	5/2002	Langer et al.	2005/0121039	A1	6/2005	Brooks et al.
6,390,096	B1	5/2002	Conrad et al.	2005/0154412	A1	7/2005	Krueger et al.
6,395,017	B1	5/2002	Dwyer et al.	2005/0171572	A1	8/2005	Martinez
6,401,717	B1	6/2002	Conrad et al.	2005/0199248	A1	9/2005	Pflueger et al.
6,415,796	B1	7/2002	Conrad et al.	2005/0267321	A1	12/2005	Shaddock
6,431,174	B1	8/2002	Knudson et al.	2005/0274384	A1	12/2005	Tran et al.
6,439,238	B1	8/2002	Brenzel et al.	2006/0150986	A1	7/2006	Roue et al.
6,450,169	B1	9/2002	Conrad et al.	2006/0201519	A1	9/2006	Frazier et al.
6,453,905	B1	9/2002	Conrad et al.	2006/0207606	A1	9/2006	Roue et al.
6,458,127	B1	10/2002	Truckai et al.	2006/0229669	A1	10/2006	Mirizzi et al.
6,467,485	B1	10/2002	Schmidt	2006/0235380	A1	10/2006	Vassallo
6,502,574	B2	1/2003	Walter et al.	2006/0260623	A1	11/2006	Brooks et al.
6,507,675	B1	1/2003	Lee et al.	2006/0289014	A1	12/2006	Purdy et al.
6,513,530	B2	2/2003	Knudson et al.	2006/0289015	A1	12/2006	Boucher et al.
6,513,531	B2	2/2003	Knudson et al.	2007/0010787	A1	1/2007	Hackett et al.
6,516,806	B2	2/2003	Knudson et al.	2007/0108077	A1	5/2007	Lung et al.
6,523,541	B2	2/2003	Knudson et al.	2007/0144534	A1	6/2007	Mery et al.
6,523,542	B2	2/2003	Knudson et al.	2007/0198040	A1	8/2007	Buevich et al.
6,530,896	B1	3/2003	Elliott	2007/0261701	A1	11/2007	Sanders
6,546,936	B2	4/2003	Knudson et al.	2007/0288057	A1	12/2007	Kuhnel
6,569,191	B1	5/2003	Hogan	2007/0295340	A1	12/2007	Buscemi
6,578,763	B1	6/2003	Brown	2008/0023012	A1	1/2008	Dineen et al.
6,601,584	B2	8/2003	Knudson et al.	2008/0027560	A1	1/2008	Jackson et al.
6,626,181	B2	9/2003	Knudson et al.	2008/0053461	A1	3/2008	Hirotsuka et al.
6,626,916	B1	9/2003	Yeung et al.	2008/0058584	A1	3/2008	Hirotsuka et al.
6,629,988	B2	10/2003	Weadock	2008/0066764	A1	3/2008	Paraschac et al.
6,634,362	B2	10/2003	Conrad et al.	2008/0066765	A1	3/2008	Paraschac et al.
6,636,767	B1	10/2003	Knudson et al.	2008/0066766	A1	3/2008	Paraschac et al.
6,703,040	B2	3/2004	Katsarava et al.	2008/0066767	A1	3/2008	Paraschac et al.
6,748,950	B2	6/2004	Clark et al.	2008/0066769	A1	3/2008	Paraschac et al.
6,748,951	B1	6/2004	Schmidt	2008/0078411	A1 *	4/2008	Buscemi
6,772,944	B2	8/2004	Brown			 A61F 5/566
6,899,105	B2	5/2005	Krueger et al.	2008/0078412	A1	4/2008	Buscemi et al.
7,017,582	B2	3/2006	Metzger et al.	2008/0082113	A1	4/2008	Bishop et al.
7,063,089	B2	6/2006	Knudson et al.	2008/0188947	A1	8/2008	Sanders
7,090,672	B2	8/2006	Underwood et al.	2009/0038623	A1	2/2009	Farbarik et al.
7,107,992	B2	9/2006	Brooks et al.	2009/0044814	A1	2/2009	Iancea et al.
D536,792	S	2/2007	Krueger et al.	2009/0084388	A1	4/2009	Bagley et al.
7,192,443	B2	3/2007	Solem et al.	2009/0126742	A1	5/2009	Summer
7,213,599	B2	5/2007	Conrad et al.	2009/0319046	A1	12/2009	Krespi et al.
7,255,110	B2	8/2007	Knudson et al.	2010/0037901	A1	2/2010	Rousseau et al.
7,322,356	B2	1/2008	Critzer et al.	2010/0132719	A1	6/2010	Jacobs et al.
7,337,781	B2	3/2008	Vassallo	2010/0158854	A1	6/2010	Puisais
7,793,661	B2	9/2010	Macken	2010/0163056	A1 *	7/2010	Tschopp et al.
7,824,704	B2	11/2010	Anderson et al.	2011/0100377	A1 *	5/2011	Weadock
7,909,037	B2	3/2011	Hegde et al.			 A61F 5/566
7,909,038	B2	3/2011	Hegde et al.	2011/0166598	A1	7/2011	Gonazles et al.
7,934,506	B2	5/2011	Woodson et al.	2011/0174315	A1	7/2011	Zhang et al.
7,947,076	B2	5/2011	Vassallo et al.	2011/0290258	A1	12/2011	Pflueger et al.
7,992,567	B2	8/2011	Hirotsuka et al.	2011/0308529	A1	12/2011	Gillis et al.
7,997,266	B2	8/2011	Frazier et al.	2011/0308530	A1	12/2011	Gillis et al.
8,167,787	B2	5/2012	Gillis	2012/0017919	A1	1/2012	Gillis
8,186,355	B2	5/2012	van der Burg et al.	2012/0132214	A1	5/2012	Gillis
8,220,466	B2	7/2012	Frazier et al.	2012/0138069	A1	6/2012	Gillis et al.
				2012/0143134	A1	6/2012	Hollis et al.
				2012/0180799	A1	7/2012	Pflueger et al.
				2013/0098374	A1	4/2013	Gillis et al.

(56)

References Cited**U.S. PATENT DOCUMENTS**

2013/0109910	A1	5/2013	Alexander et al.
2013/0233324	A1	9/2013	Witt et al.
2014/0000631	A1	1/2014	Gillis et al.
2014/0007885	A1	1/2014	Gillis et al.
2014/0014116	A1	1/2014	Gillis et al.
2015/0202074	A1	7/2015	Gillis et al.

FOREIGN PATENT DOCUMENTS

JP	05-337126	A	12/1993
JP	2604833		1/1997
JP	2001198147		7/2001
JP	2006507038		3/2006
JP	2007-97706		4/2007
JP	2007-512090		5/2007
JP	2007229485		9/2007
JP	2007525277	A	9/2007
WO	WO 97/18854	A1	5/1997
WO	WO 99/00058	A1	1/1999
WO	WO 00/66050	A1	11/2000
WO	WO 01/89426	A1	11/2001
WO	WO 02/13738	A1	2/2002
WO	WO 02/076341	A2	10/2002
WO	WO 02/076352	A1	10/2002
WO	WO 02/076353	A1	10/2002
WO	WO 02/076354	A1	10/2002
WO	WO 03/041612	A2	5/2003
WO	WO 03/055417	A1	7/2003
WO	WO 03/065947	A1	8/2003
WO	WO 2005/044158	A1	5/2005
WO	WO 2006/012188	A1	2/2006
WO	WO 2006/093533	A1	9/2006
WO	WO 2006/101610	A2	9/2006
WO	WO 2007/056583	A1	5/2007
WO	WO 2007/070024	A2	6/2007
WO	WO 2008/042058	A1	4/2008

WO	WO 2008/097890	A2	8/2008
WO	WO 2009/032625	A1	3/2009
WO	WO 2010/028036	A1	3/2010
WO	WO 2010/045546	A1	4/2010
WO	WO 2010/051195	A1	5/2010

OTHER PUBLICATIONS

Gillis; U.S. Appl. No. 14/282,943 entitled "Partially erodable systems for treatment of obstructive sleep apnea," filed May 20, 2014.

DeRowe et al.; A minimally invasive technique for tongue base stablation in obstructive sleep apnea; Operative Techniques in Otolaryngology-Head and Neck Surgery; 11(1); pp. 41-46; Mar. 2000.

Jeon et al.; Shape memory and nonostructure in poly(norbornyl-POSS) copolymers; Polym Int; vol. 49(5); pp. 453-457; May 2000.

Lui et al.; Thermomechanical characterization of a tailored series of shape memory polymers; J Applied Med Polymers; vol. 6/ No. 2; pp. 47-52; Sep. 2002.

Mather et al.; Strain recovery in POSS hybrid thermoplastics; Polymer Preprints; vol. 41, No. 1; pp. 528-529; (year of pub. sufficiently earlier than effective US filed and any foreign priority date) 2000.

Miller et al.; Role of the tongue base suspension suture with the Repose System bone screw in multilevel surgical management of obstructive sleep apnea; Otolaryngol Head Neck Surg.; 126(4); pp. 392-398; Apr. 2002.

Walker et al.; Palatal implants for snoring and sleep apnea; Operative Techniques in otolaryngology; 17(4); pp. 238-241; Dec. 2006.

Woodson et al.; Pharyngeal suspension suture with Repose bone screw for obstructive sleep apnea; Otolaryngol Head Neck Surg.; 122(3); pp. 395-401; Mar. 2000.

Rampersaud et al.; U.S. Appl. No. 14/340,324 entitled "Systems and methods for treatment of an airway disorder," filed Jul. 24, 2014.

Collins English Dictionary; "elastomer" (definition); Complete & Unabridged; 10th Edition; HarperCollins Publishers; May 11, 2015; retrieved from the internet (<http://dictionary.reference.com/browse/elastomeric>).

* cited by examiner

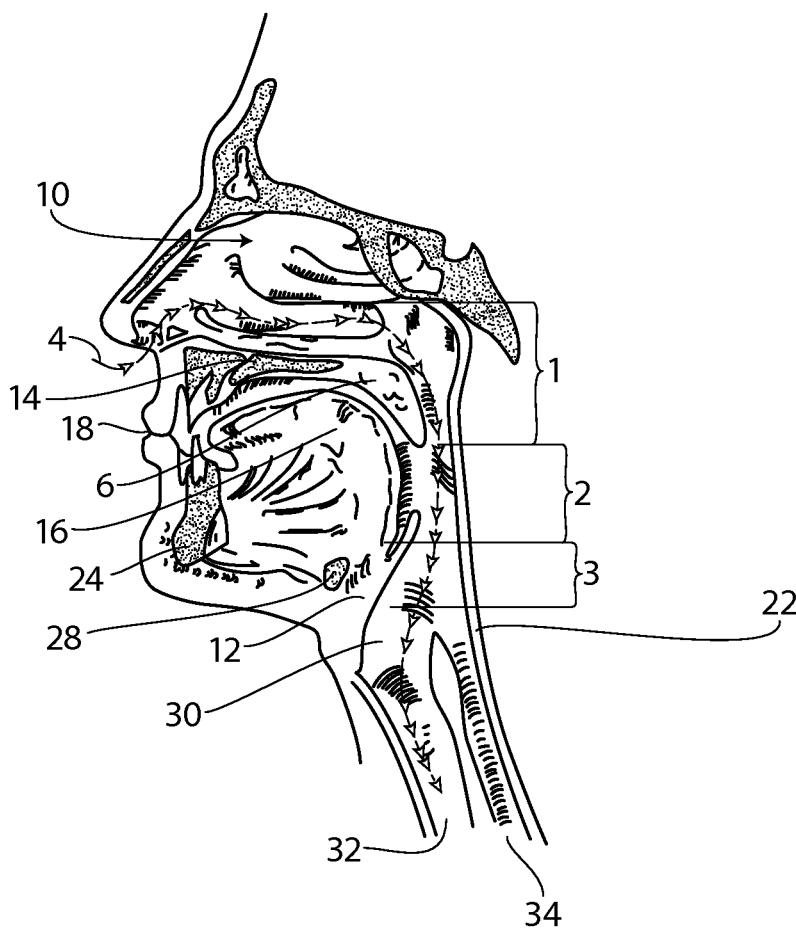


FIG. 1

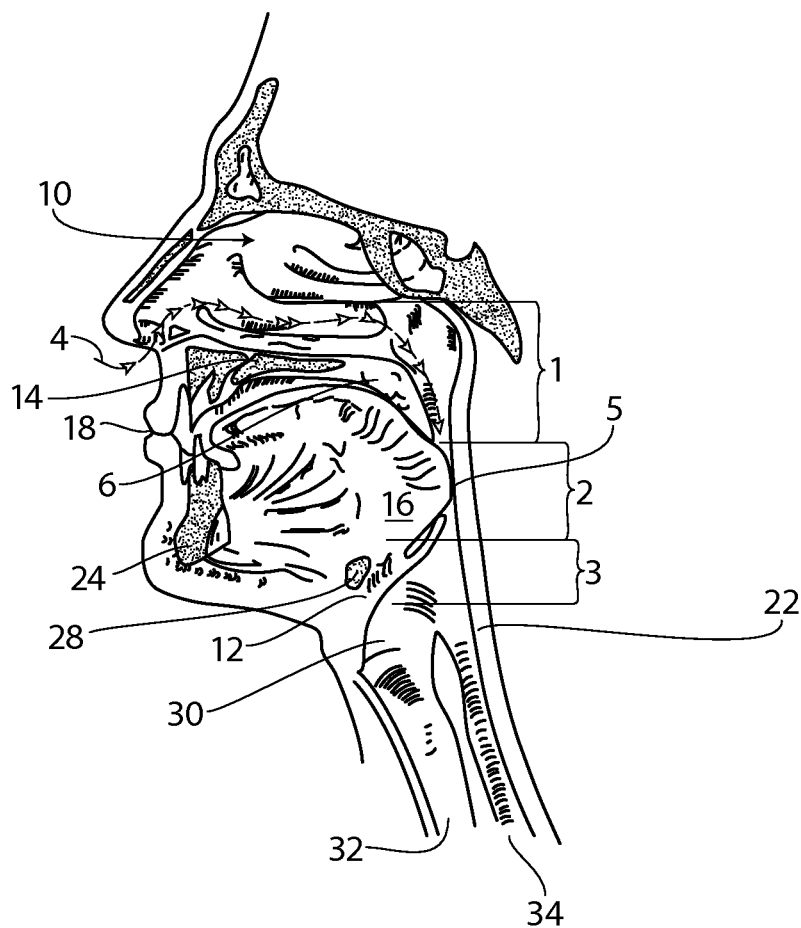


FIG. 2A

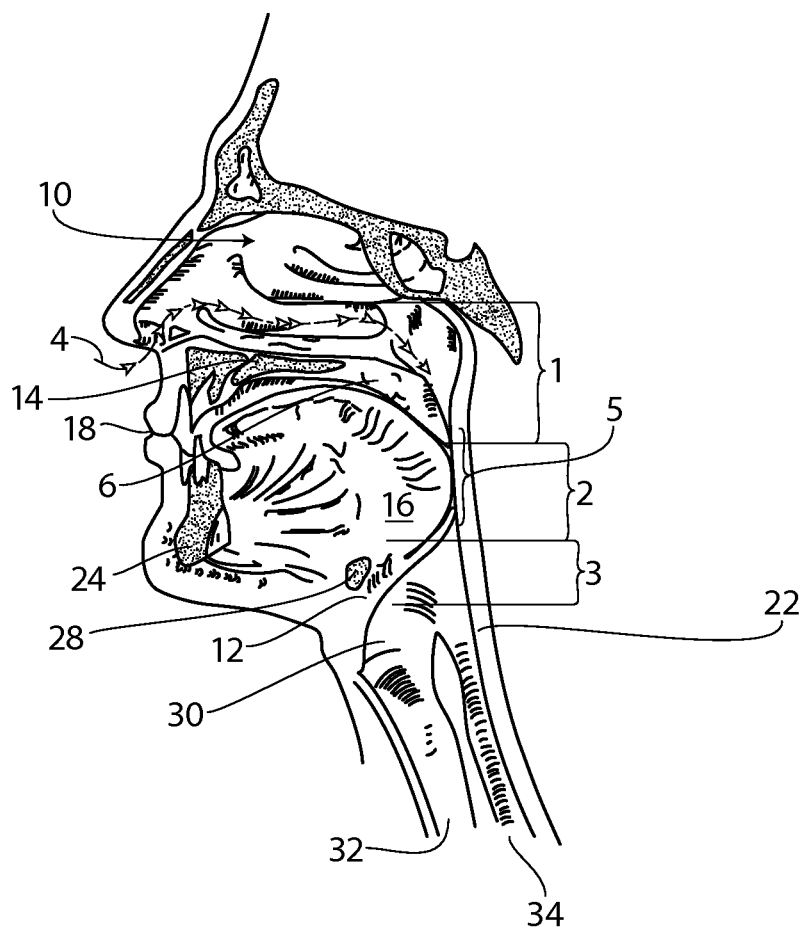


FIG. 2B

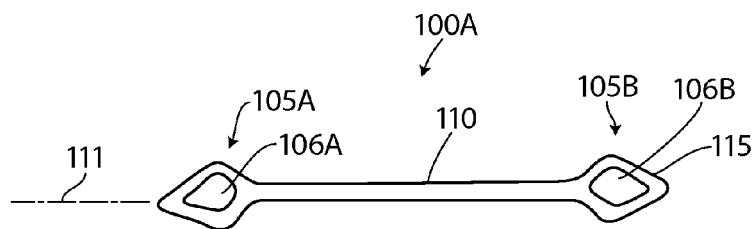


FIG. 3A

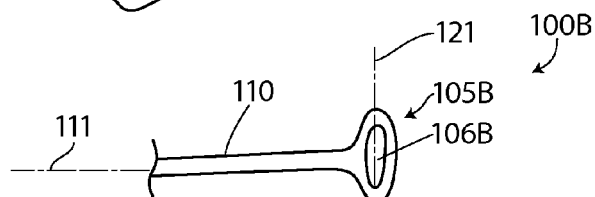


FIG. 3C

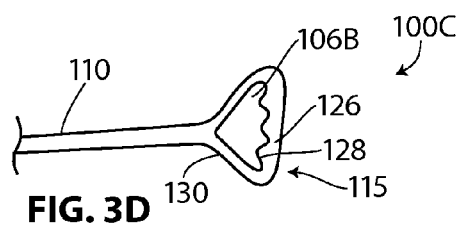


FIG. 3D

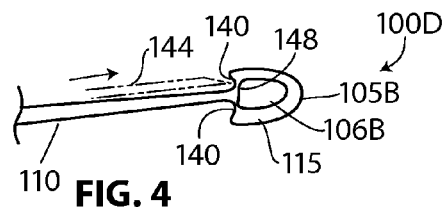


FIG. 4

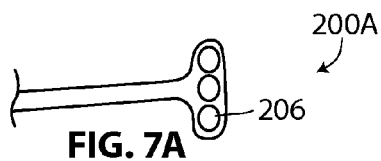


FIG. 7A

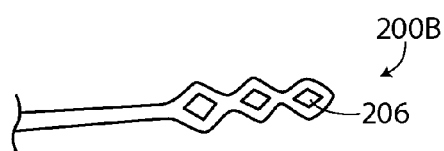


FIG. 7B

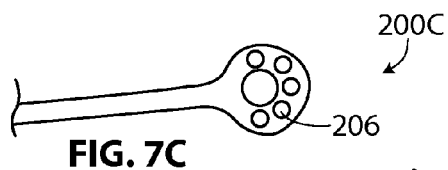


FIG. 7C

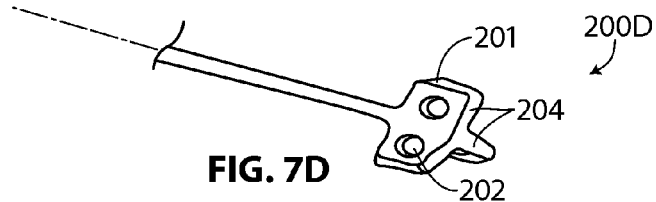


FIG. 7D

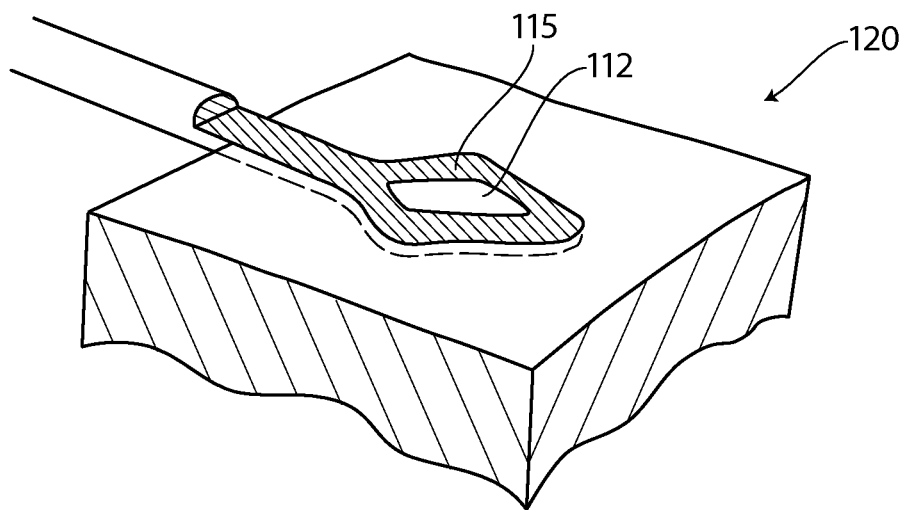


FIG. 3B

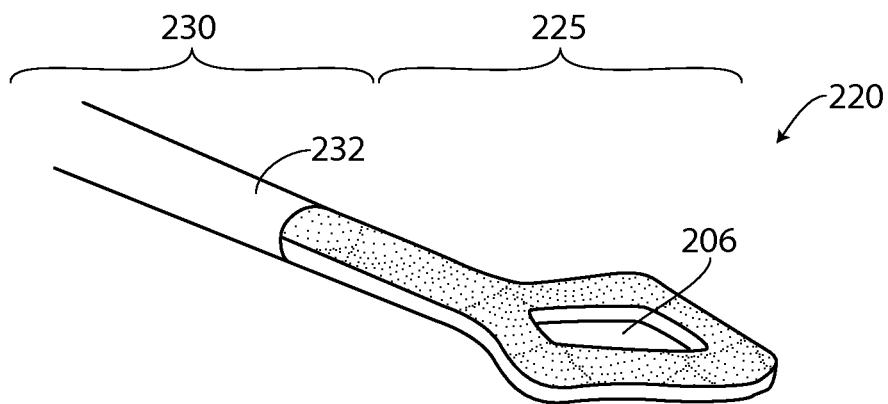


FIG. 9

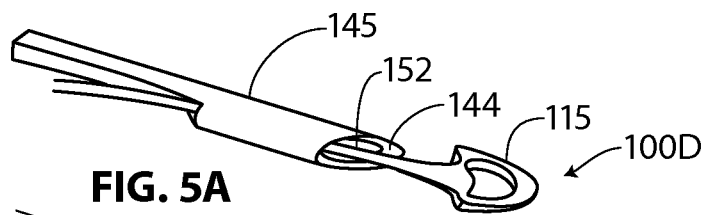


FIG. 5A

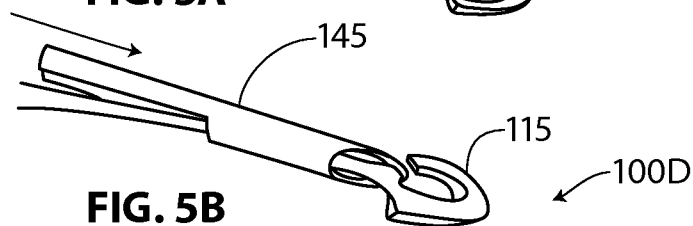


FIG. 5B

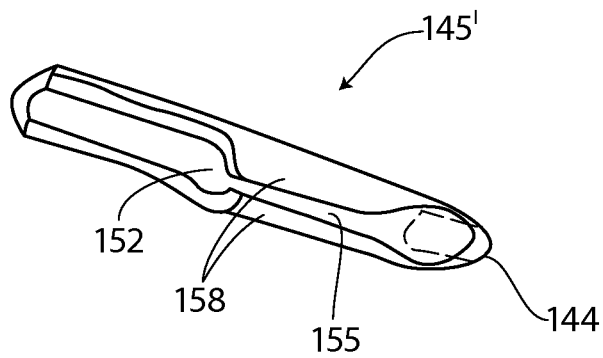


FIG. 6

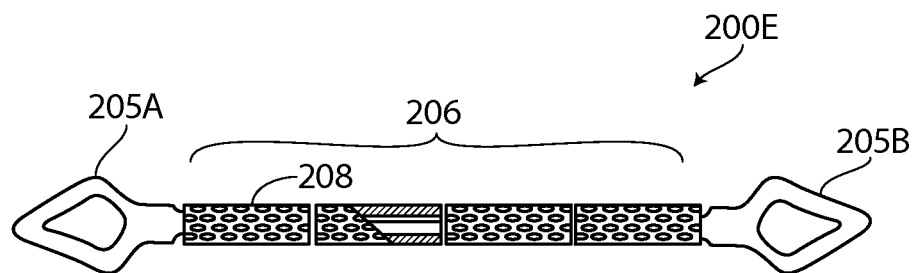
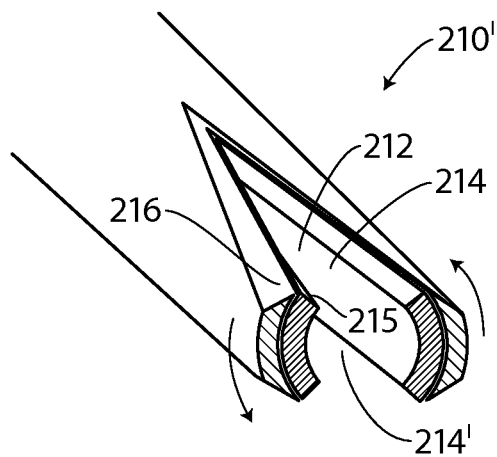
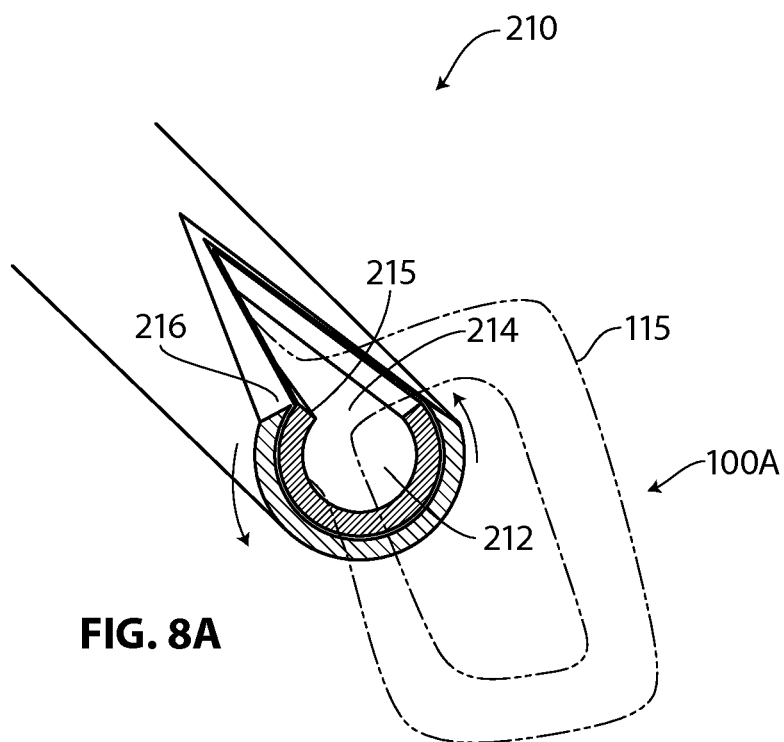


FIG. 7E



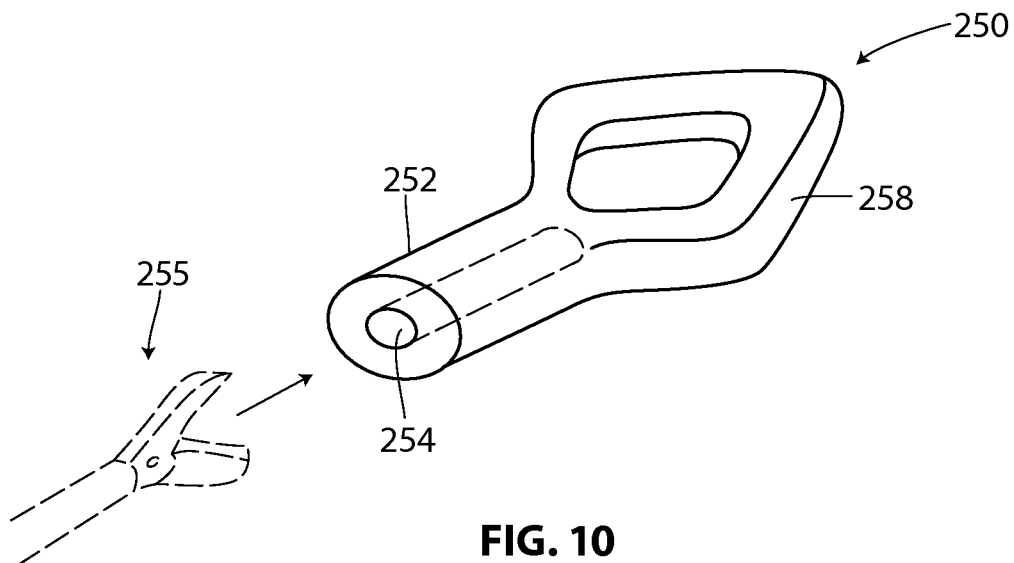


FIG. 10

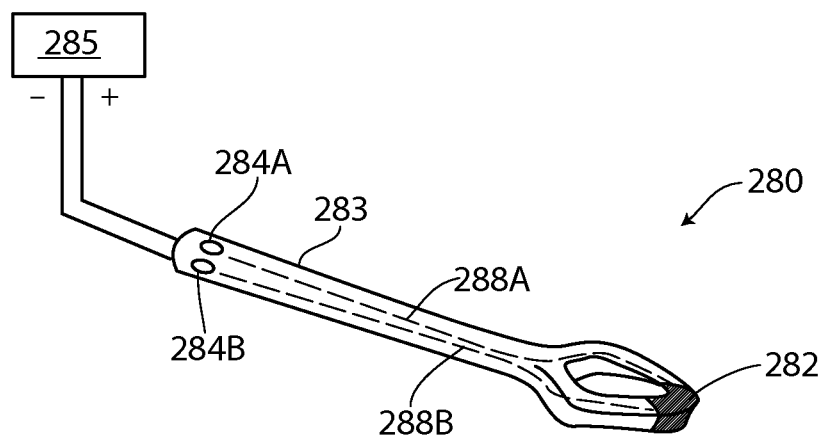


FIG. 11

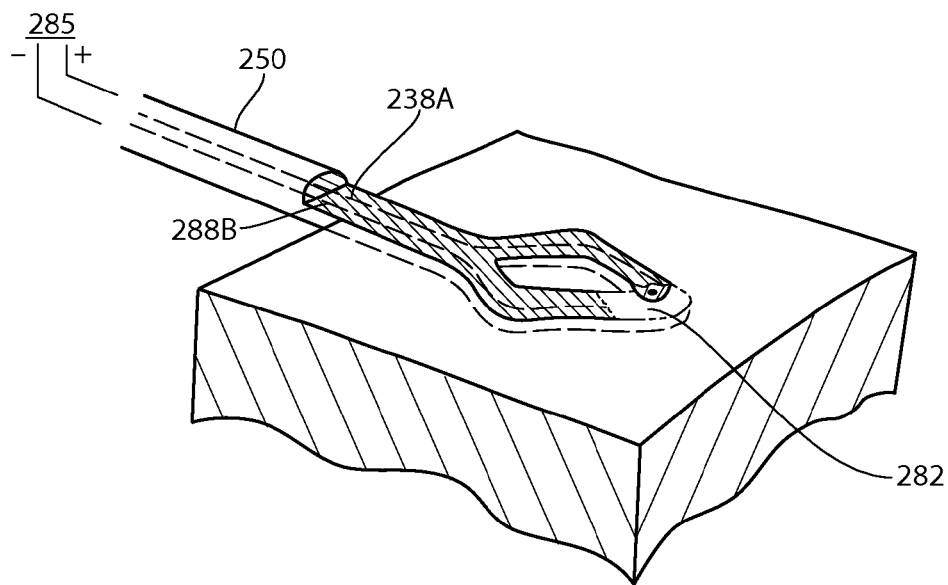


FIG. 12

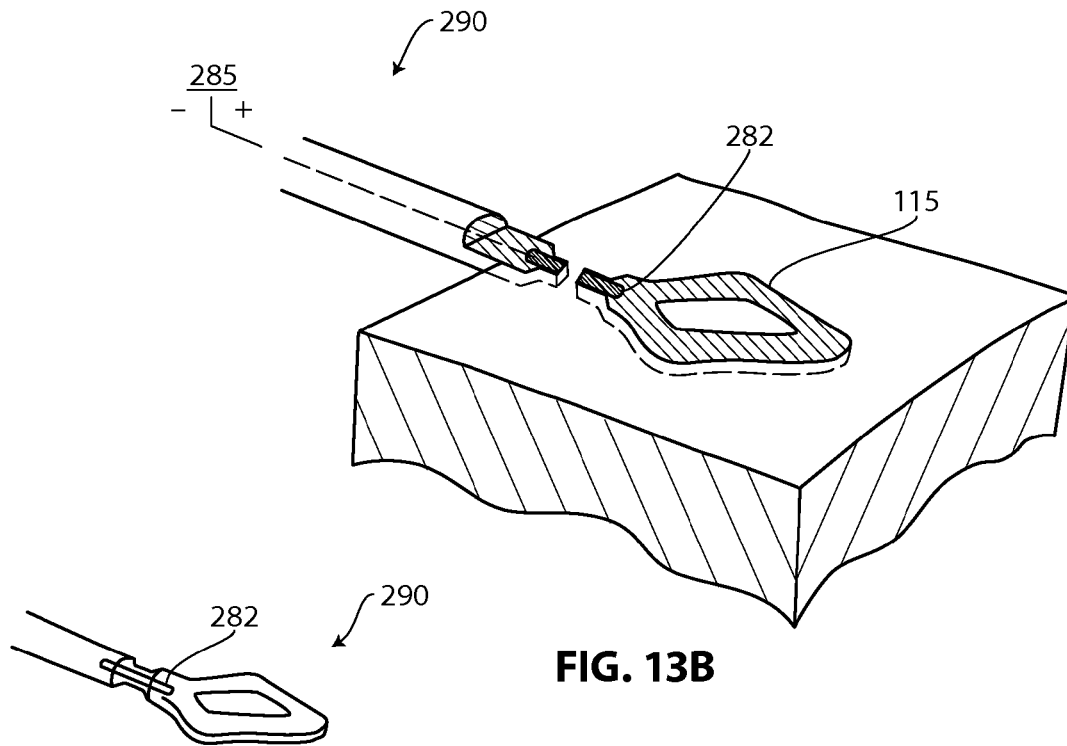


FIG. 13B

FIG. 13A

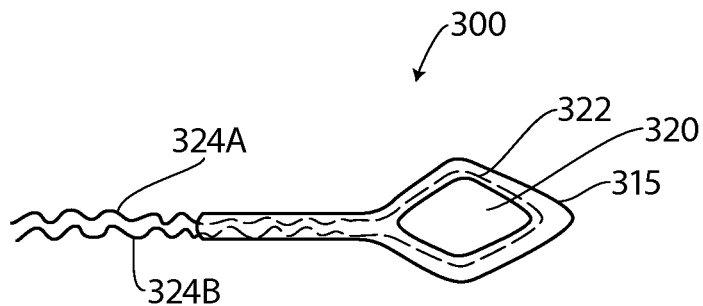


FIG. 14

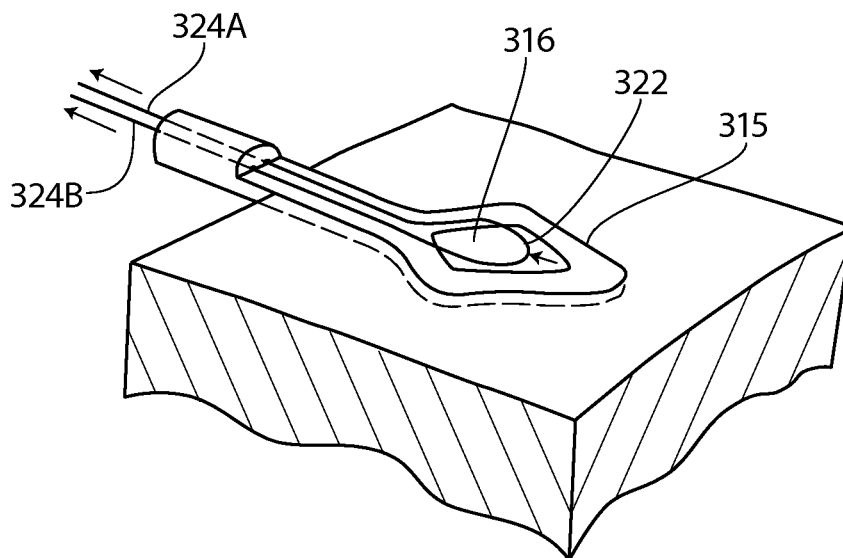


FIG. 15

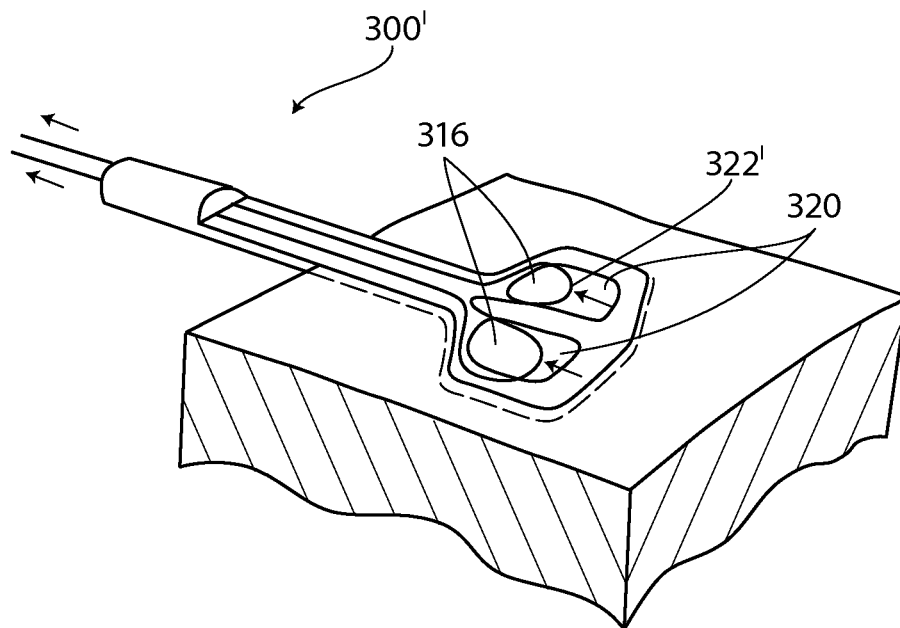
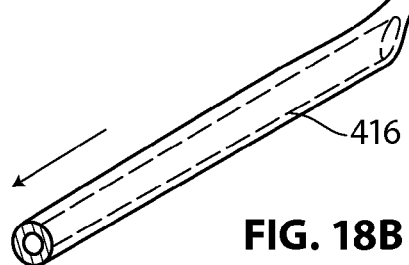
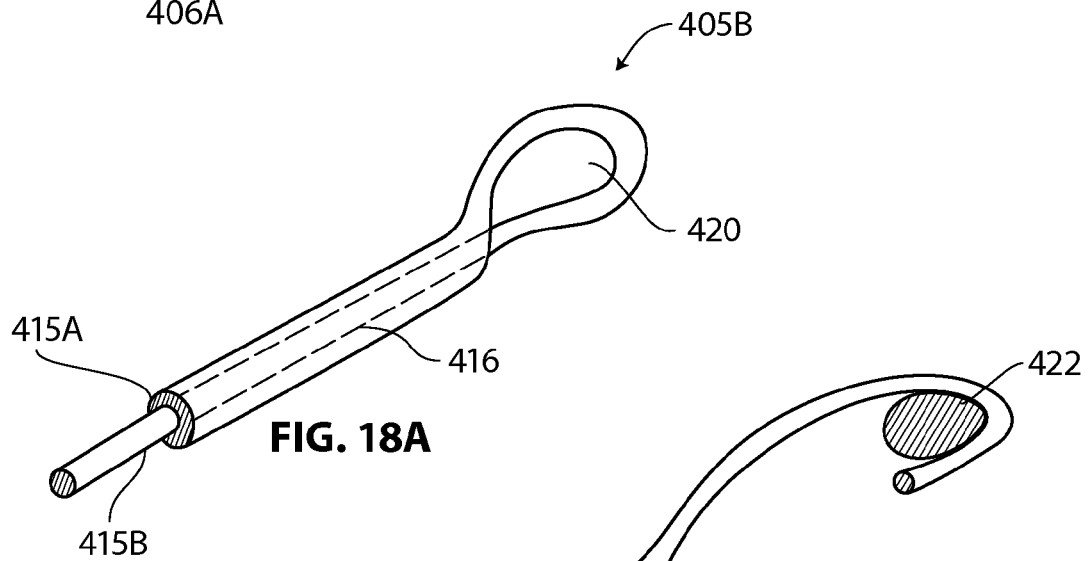
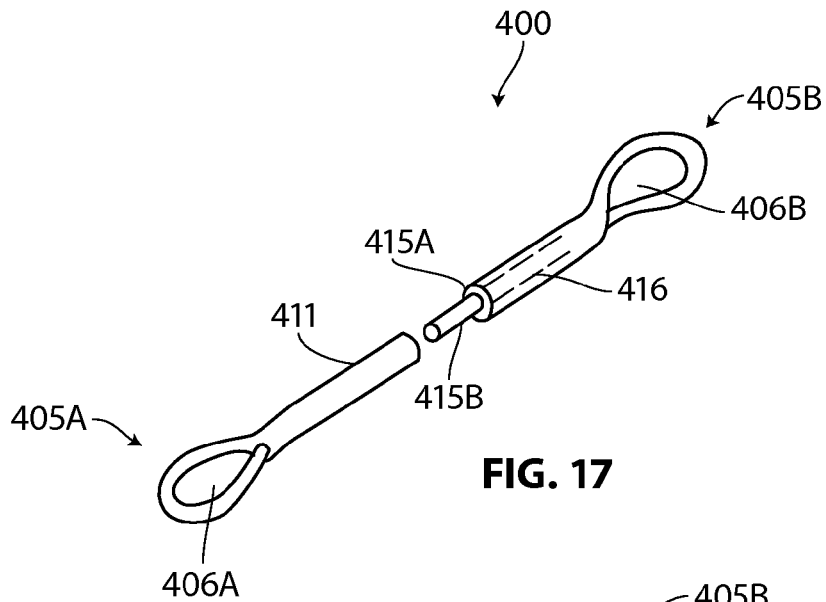


FIG. 16



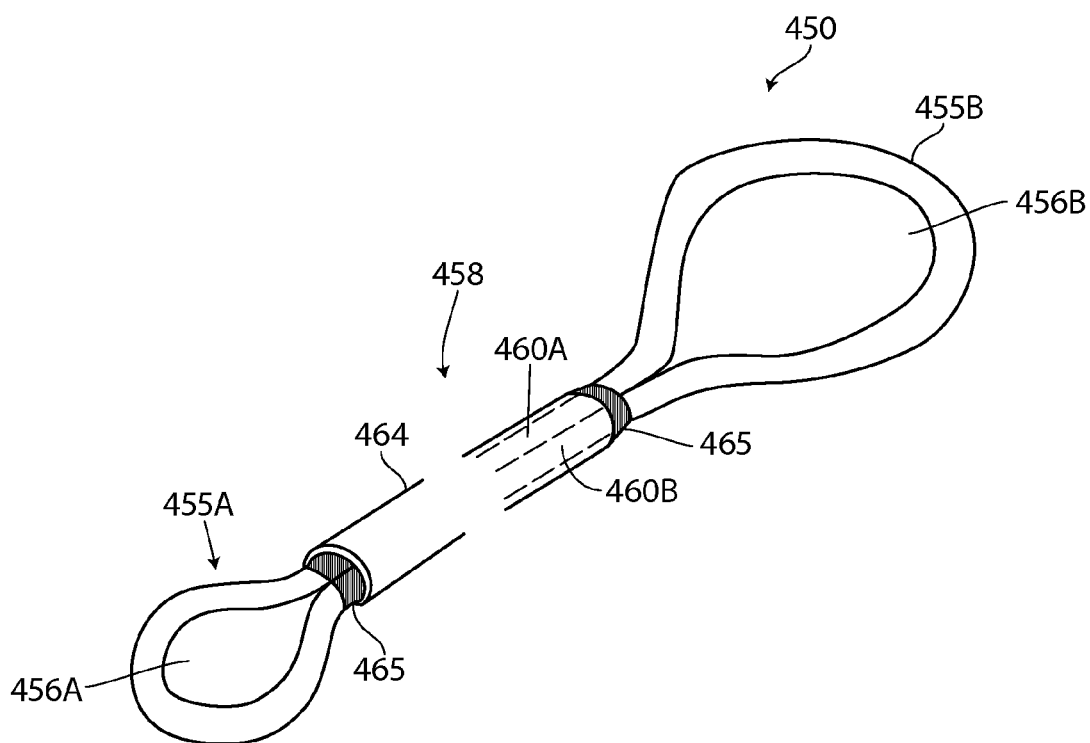


FIG. 19

SYSTEMS AND METHODS FOR TREATMENT OF SLEEP APNEA

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a divisional of U.S. application Ser. No. 13/053,025, filed Mar. 21, 2011, now U.S. Pat. No. 8,776,799, which claims priority to: U.S. Provisional Application No. 61/315,835, filed Mar. 19, 2010; U.S. Provisional Application No. 61/315,838, filed Mar. 19, 2010; U.S. Provisional Application No. 61/347,348, filed May 21, 2010; U.S. Provisional Application No. 61/347,356, filed May 21, 2010; U.S. Provisional Application No. 61/367,707, filed Jul. 26, 2010; U.S. Provisional Application No. 61/418,238, filed Nov. 30, 2010; U.S. Provisional Application No. 61/419,690, filed Dec. 3, 2010, each of which is herein incorporated by reference in its entirety.

INCORPORATION BY REFERENCE

All publications and patent applications mentioned in this specification are herein incorporated by reference to the same extent as if each individual publication or patent application was specifically and individually indicated to be incorporated by reference.

FIELD

The invention relates to the field of methods and devices for the treatment of obstructive sleep apnea, and more particularly to opening the airway of subjects with symptoms of obstructive sleep apnea.

BACKGROUND

Sleep apnea is defined as the cessation of breathing for ten seconds or longer during sleep. During normal sleep, the throat muscles relax and the airway narrows. During the sleep of a subject with obstructive sleep apnea (OSA), the upper airway narrows significantly more than normal, and during an apneic event, undergoes a complete collapse that stops airflow. In response to a lack of airflow, the subject is awakened at least to a degree sufficient to reinitiate breathing. Apneic events and the associated arousals can occur up to hundreds of times per night, and become highly disruptive of sleep. Obstructive sleep apnea is commonly but not exclusively associated with a heavy body type, a consequence of which is a narrowed oropharyngeal airway.

Cyclic oxygen desaturation and fragmented sleeping patterns lead to daytime sleepiness, the hallmark symptom of the disorder. Further consequences of sleep apnea may include chronic headaches and depression, as well as diminished facilities such as vigilance, concentration, memory, executive function, and physical dexterity. Ultimately, sleep apnea is highly correlated with increased mortality and life threatening co morbidities. Cardiology complications include hypertension, congestive heart failure, coronary artery disease, cardiac arrhythmias, and atrial fibrillation. OSA is a highly prevalent disease condition in the United States. An estimated 18 million Americans suffer from OSA to degrees that range from mild to severe, many of whom are undiagnosed, at least in part because the afflicted subjects are often unaware of their own condition.

Treatment of OSA usually begins with suggested lifestyle changes, including weight loss and attention to sleeping habits (such as sleep position and pillow position), or the use of

oral appliances that can be worn at night, and help position the tongue away from the back of the airway. More aggressive physical interventions include the use of breathing assist systems that provide a positive pressure to the airway through a mask that the subject wears, and which is connected to a breathing machine. In some cases, pharmaceutical interventions can be helpful, but they generally are directed toward countering daytime sleepiness, and do not address the root cause. Some surgical interventions are available, such as nasal surgeries, tonsillectomy and/or adenoidectomy, reductions in the soft palate, uvula or the tongue base, or advancing the tongue base by an attachment to the mandible and pulling the base forward. These surgical approaches can be quite invasive and thus have a last-resort aspect to them, and further, simply do not reliably alleviate or cure the condition. There is a need for less invasive procedures that show promise for greater therapeutic reliability. There is additional need for the ability to reverse procedures or otherwise revise the procedure, thus allowing for the ability to reverse or otherwise revise the effects of the procedure due to side effects or other undesirable outcomes which may result from the procedure. Additionally, there is the need to do these procedural reversals or revisions in a manner that does not require excessive tissue cutting or invasiveness which can act as a deterrent for patients or physicians to perform such a revision procedure.

SUMMARY OF THE DISCLOSURE

The invention relates to a method of alleviating obstructive collapse of airway-forming tissues, and for devices with which to implement the method. Typical patients for whom the method and device may provide therapeutic benefit are those who suffer from obstructive sleep apnea. The method includes implanting a device at a site in the tissue and bioeroding the bioerodible portion of the device to change the shape of the device and to remodel the airway-forming tissue. The implanted device is sized and shaped to conform to the airway-forming tissue site in a manner compatible with normal physiological function of the site; and includes a resiliently deformable portion and a bioerodible portion. In, typical embodiments of the method, remodeling the airway-forming tissue results in the airway being unobstructed during sleep, and further, typically, the thus-unobstructed airway diminishes the frequency of apneic events. Remodeling may include reshaping or otherwise altering the position or conformation of airway associated tissue so that its tendency to collapse during sleep is diminished.

The airway is formed from various tissues along its length from the mouth to the lungs. Embodiments of the method include implanting a flexible implant, such as an elastomeric device, into any one or more of these tissues, including, for example, the soft palate, the tongue, generally the base of the tongue, and the pharyngeal walls, typically the posterior and lateral portions of the pharyngeal wall.

In some embodiments, the device is in a deformed shape when implanted, and a bioerodable portion erodes to thereby release a tensioned shape of the implant to apply retraction forces to the site.

With regard to the bioeroding of the bioerodible portion of the device, this may occur over a time span that ranges from days to months. In some embodiments, the bioeroding proceeds at a rate that correlates with the ratio of the biologically-exposed surface area of the bioerodible portion to the volume of the bioerodible portion.

In some embodiments of the method, the bioerosion occurs at a rate that is sufficiently slow for the tissue site to recover from the implanting prior to the device substantially changing

shape. In some of these embodiments, the recovery of the tissue site includes a forming of fibrotic tissue around the device, which typically stabilizes the device in the site, and provides the device greater leverage with which to reform the shape of the implant site and its surrounding tissue. In some embodiments, after implanting, and as part of the healing response or recovery from the implantation wound, the newly formed fibrotic tissues infiltrates into holes, pores, or interstices in the device. In some embodiments of the method, a bioactive agent, previously incorporated into the bioerodible material, is released or eluted from the bioerodible portion of the device as it is eroding.

In another aspect of the methods described herein, a method of forming a device to alleviate obstructive collapse of an airway during sleep is provided. The method includes forming a resiliently deformable material into an initial shape that corresponds to the preferred shape of the device, the initial shape having a site for accommodating bioerodible material; changing the initial shape of the resiliently deformable material into a non-preferred shape that is sized and configured into an implantable shape that conforms to on airway-forming tissue site and is compatible with normal physiological function after implantation; and stabilizing the implantable shape by incorporating the bioerodible material into the accommodating site. In some of these method embodiments, changing the initial shape of the resiliently deformable material includes absorbing a force sufficient to remodel the airway as the force is transferred from the device into an implant site after implantation of the device. That level of force is further typically insufficient to remodel the airway to an extent that it is unable to move in a manner that allows substantially normal or acceptable physiological function of the airway.

As noted above, some aspects of the invention further provide a device for alleviating obstruction in an airway, such obstruction typically occurring during sleep. Embodiments of the device include an implantable device sized and shaped to conform to an airway-forming tissue site in a manner compatible with normal physiological function of the site, the device including a resiliently deformable portion and a bioerodible portion. In these embodiments, the resiliently deformable portion has a preferred shape that is constrained in a deformed shape by the bioerodible portion, and the device is configured to return toward the preferred shape of the resiliently deformable portion upon erosion of the bioerodible portion. In some embodiments, the preferred configuration is adapted to remodel the shape of the airway so as to provide a more open airway during sleep.

In typical embodiments of the device, the resiliently deformable portion may include any one or more of a metal or a polymer. In these embodiments, a resiliently deformable metal may include any one or more of stainless steel, spring steel, or superelastic nickel-titanium alloy, and a resiliently deformable polymer may include any one or more of silicon rubber, polyesters, polyurethanes, or polyolefins. In some embodiments, the bioerodible portion may include any one or more of polycaprolactone, polylactic acid, polyglycolic acid, polylactide coglycolide, polyglactin, poly-L-lactide, polyhydroxalkanoates, starch, cellulose, chitosan, or structural protein.

Some embodiments of the device include a portion adapted to engage the tissue into which it is implanted, and in some of these embodiments, the so-adapted portion includes a site for tissue in-growth, such in-growth serving to keep the device and tissue in close proximity, serving to promote implant site remodeling in a manner that conforms to the changing shape of the device. Finally, in some embodiments, the implantable

device is configured with sufficient elasticity to allow normal physiological movement around an airway-forming tissue implant site when the device is implanted in the implant site.

In other embodiments, the adapted portion contains sites for tissue to link through the implant after implantation forming tissue plugs which thus form an attachment between the implant and the adjacent tissue without a corresponding adhesion of tissue to the implant. This type of arrangement can produce an implant that can effectively attach to and move tissue while remaining easily removable from the tissue. The tissue plugs can be formed by linking the implant around an encircled or surrounded mass of tissue or allowing tissue to heal through the implant thus forming the island of encircled or surrounded tissue. Implants can contain one or more surrounded masses of tissue allowing attachment to the adjacent tissue. In some embodiments, a proximal end of the implant is anchored to the patient's mandible and a distal end or ends of the implant is/are releasably anchored to one or more tissue plugs.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 provides an overview of the healthy human airway anatomy, with particular attention to the nasopharyngeal, oropharyngeal, and hypopharyngeal regions.

FIG. 2A provides a view of a compromised airway, with an occlusion in the oropharyngeal region due to posterior slipage of the base of the tongue.

FIG. 2B provides a view of a compromised airway with palate closure.

FIG. 3A depicts an elongate implant component of a revisable OSA implant system, the implant having end portions with openings for growth of a tissue plug therethrough to secure the end portions in a treatment site.

FIG. 3B is a cut-away view of an end portion of the implant of FIG. 3A in a tissue site.

FIG. 3C depicts another elongate implant embodiment similar to that of FIG. 3A.

FIG. 3D depicts another elongate implant embodiment.

FIG. 4 depicts another elongate implant corresponding to aspects of the invention.

FIG. 5A depicts a second component of a revisable OSA implant system, the second component comprising a cutting tool.

FIG. 5B depicts the cutting tool of FIG. 5A in a method of use.

FIG. 6 depicts an alternative cutting tool similar to that of FIGS. 5A-5B.

FIG. 7A depicts another elongate implant corresponding to aspects of the invention.

FIG. 7B depicts another elongate implant embodiment.

FIG. 7C depicts another elongate implant embodiment.

FIG. 7D depicts another elongate implant embodiment with multiple openings in multiple planes.

FIG. 7E is a partially cut-away view that depicts an OSA implant with an elastomeric portion that is configured for being releasably maintained in a tensioned or non-repose condition by a magnesium or magnesium alloy biodissolvable material or element.

FIG. 8A depicts the working end of another embodiment of a cutting tool for cutting a portion of an implant in situ.

FIG. 8B depicts another embodiment of a cutting tool for cutting an implant in a revision procedure.

FIG. 9 depicts another implant with a medial portion having a surface configured for low adhesive energy.

FIG. 10 depicts another elongate implant corresponding to aspects of the invention.

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FIG. 11 depicts another implant corresponding to aspects of the invention including a sacrificial portion that can be sacrificed in response to an external stimulus.

FIG. 12 is a cut-away view depicting the implant of FIG. 11 in a tissue site after actuation of the sacrificial portion of the implant.

FIG. 13A depicts an alternative implant including an electrolytically sacrificial portion that can be sacrificed in response to a direct current.

FIG. 13B is a cut-away view depicting the implant of FIG. 13A in a tissue site after actuation of electrolytic connection portion of the implant.

FIG. 14 depicts an end portion of an alternative revisable implant including a cut wire for cutting a tissue plug.

FIG. 15 is a cut-away view depicting the implant of FIG. 14 in a tissue site in the process of actuating the cut wire.

FIG. 16 depicts an end portion of an alternative revisable implant including a cut wire for cutting a plurality of tissue plugs.

FIG. 17 depicts an alternative revisable OSA implant.

FIGS. 18A and 18B illustrate an end portion of the revisable implant of FIG. 17.

FIG. 19 depicts an alternative revisable OSA implant.

DETAILED DESCRIPTION

A. Anatomy of the Pharynx

FIG. 1 is a sagittal view of the structures that form the pharyngeal airway 4; some of these structures can become compromised under various conditions to the extent that they obstruct or occlude passage of air through the airway 4, and thus contribute to obstructive sleep apnea. The pharynx is divided, from superior to inferior, into the nasopharynx 1, the oropharynx 2 and the hypopharynx 3. Variations of FIG. 1 are provided in FIGS. 2A and 2B which depict airway obstruction sites 5 at various levels in the pharyngeal airway. FIG. 2A, for example, shows an occlusion 5 at the level of the oropharynx 2, where the base of the tongue 16 and a thickened posterior pharyngeal wall 22 have collapsed against each other. FIG. 2B provides a view of a compromised airway with palate closure. It is also possible for airway obstruction to occur at the level of the nasopharynx 1, where an elongated and/or floppy soft palate can collapse against a thickened posterior pharyngeal wall. Further, an obstruction can occur at the level of the hypopharynx 3, where both an elongated soft palate and a floppy epiglottis 12 can collapse against the pharyngeal wall 22.

With reference to FIGS. 1-2B, the nasopharynx 1 is the portion of the pharynx at the level of or above the soft palate 6. In the nasopharynx, a deviated nasal septum or enlarged nasal turbinates may occasionally contribute to upper airway resistance or blockage. Rarely, a nasal mass, such as a polyp, cyst or tumor may be a source of obstruction. The oropharynx 2 includes structures from the soft palate 6 to the upper border of the epiglottis 12 and includes the inferior surface of the hard palate 14, tongue 16, posterior pharyngeal wall 22 and the mandible 24. The mandible typically has a bone thickness of about 5 mm to about 10 mm anteriorly with similar thicknesses laterally. An obstruction in the oropharynx 2 may result when the tongue 16 is displaced posteriorly during sleep as a consequence of reduced muscle activity during deep or non-REM sleep. The displaced tongue 16 may push the soft palate 6 posteriorly and may seal off the nasopharynx 1 from the oropharynx 2. The tongue 16 may also contact the posterior pharyngeal wall 22, which causes further airway obstruction.

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The hypopharynx 3 includes the region from the upper border of the epiglottis 12 to the inferior border of the cricoid cartilage. The hypopharynx 3 further includes the hyoid bone 28, a U-shaped, free-floating bone that does not articulate with any other bone. The hyoid bone 28 is attached to surrounding structures by various muscles and connective tissues. The hyoid bone 28 lies inferior to the tongue 16 and superior to the thyroid cartilage 30. A thyrohyoid membrane and a thyrohyoid muscle attach to the inferior border of the hyoid 28 and the superior border of the thyroid cartilage 30. The epiglottis 12 is infero-posterior to the hyoid bone 28 and attaches to the hyoid bone by a median hyoepiglottic ligament. The hyoid bone attaches anteriorly to the infero-posterior aspect of the mandible 24 by the geniohyoid muscle. Below the hypopharynx 3, the trachea 32 and esophagus 34 are also shown.

B. Revisable OSA Implants

FIG. 3A depicts a first component in an exemplary embodiment of a kit or system that provides revisable implants for treating airway disorders or obstructive sleep apnea (OSA). The second component of the exemplary kit is an introducer for insertion into a treatment site as is known in the art and co-pending applications. In FIG. 3A, an elongate device or implant body 100A has first and second end portions 105A and 105B with through-openings 106A and 106B therein. The medial portion 110 of the implant body 100A extends along axis 111 and comprises a biocompatible elastomeric material such as a silicone. The mean cross-section of the medial body portion 110 can range from 1 to 10 mm² and can be round, oval, flat, polygonal or other suitable shapes. In some embodiments, the elastic modulus of the medial portion can range from 0.5 to 10 MPA and is configured for implanting in the patient's airway tissue in a releasable, tensioned position, as described in co-pending U.S. patent application Ser. No. 11/969,201 which is incorporated herein by this reference.

Referring to FIGS. 3A and 3B, it can be seen that through-openings 106A and 106B in the implant body 100A are configured for growth of a tissue plug 112 through the opening to thereby secure the first and second end portions 105A and 105B in a selected tissue, site. The cut-away view of FIG. 3B schematically illustrates that a tissue plug 112 that grows through the opening is thus surrounded or encircled by an encircling body portion 115 of the implant. The encircling body portion 115 comprises a small cross-section element that can be cut, severed, sacrificed, decoupled, or dissolved to disengage the implant from a tissue site 120 as will be described below. The element can be a polymer or other material. In other embodiments described below, the tissue plug 112 can be cut or severed to disengage the implant from the tissue site 120. In one embodiment, the mean cross-section of the tissue plug 112, and thus the dimension across an opening 106A or 106B, can range from about 0.5 mm to 10 mm or more. The openings 106A or 106B can have a round shape in plan view or any other plan shape. The end portions 105A and 105B can have similar or dissimilar configurations, for example an implant configured for treatment of a patient's tongue may have a substantially larger end portion and opening 106B for the base of the tongue and a smaller end portion near the mandible.

FIG. 3C illustrates another implant body 100B with an end portion 105B having an elongated opening 106B through which tissue will grow to form a tissue plug to secure the end portion in the site. For example, the implant body 100B of FIG. 3C has an opening 106B with a primary axis 121 and larger dimension that extends generally orthogonal to the axis 111 of medial portion 110 of the implant body. In use, the

greater dimension of the tissue plug will better resist the retraction forces applied to tissue by the elastomeric medial portion **110** of the implant aligned with axis **111**.

FIG. 3D depicts another embodiment **100C** of a revisable implant for treating an airway disorder that is similar to that of FIG. 3C except the end portion **105B** has a through-opening **106B** with a terminal part **126** of encircling portion **115** configured with irregular shaped surface features **128** that can interface with the tissue plug that grows through opening **106B**. The surface features can comprise undulations, textures, protrusions, bumps and the like that can assist in maintaining the end portion in a fixed position when under the tensioning or retraction forces applied by the medial portion **110** of the implant body **100C**. In the implant body **100C** of FIG. 3D, the end portion **105B** also can have an encircling element **115** that includes a proximal portion **130** of a lower modulus material similar to the modulus of medial portion **110** and the terminal part **126** having a higher modulus to prevent its deformation under tensioning forces.

FIG. 4 depicts another embodiment **100D** of a revisable implant that is similar to previous embodiments except that at least one end portion **105B** includes an indent feature **140** in the proximal-facing aspect of the encircling portion **115** wherein the indent feature **140** is adapted to direct and receive a cutting blade or edge **144** (phantom view) of a cutting tool for cutting the encircling portion of the implant body to allow its removal from the treatment site. As will be described below (with reference to FIG. 5B), a cutting tool **145** can be advanced along the medial portion **110** of the implant to sever the end portion, which then will allow the entire implant to be withdrawn from the implant site. In another aspect of the invention, the indent feature **140** in the encircling portion **115** can direct the cutting edge **144** to a reduced cross section portion **148** that will require limited force to cut the polymer element with the cutting edge **144**.

FIGS. 5A and 5B illustrate a second component of an exemplary kit of a revisable OSA implant system wherein the tool **145** comprises an elongate member with a distal cutting edge **144**. One tool embodiment has a passageway **152** extending therethrough for receiving the elongate implant body **100D**. In using this tool **145**, a first end of the implant body would be freed from tissue or cut and then threaded through the passageway **152**. Thereafter, as depicted in FIG. 5B, the tool **145** can be advanced distally while holding the proximal end of the implant to cause the cutting edge **144** to cut across the encircling portion **115**. In FIG. 5B, it can be understood how the indent feature **140** and reduced cross section portion **148** (see FIG. 4) direct the cutting edge **144** to easily cut the element to thus release the implant from encircling the tissue plug **112** (cf. FIG. 3B). The tool **145** can be a rigid or semi-rigid member such as a hypotube with a sharpened end. The tool also can be a deflectable, articulatable or steerable member as is known in the art. In another embodiment, the tool can be a flexible plastic material with a blade insert to provide the cutting edge **144**. Referring to FIGS. 5B and 3B, it can be understood that the cut end is flexible and can be pulled from around the tissue plug to extract the implant from the site **120** (see FIG. 3B).

FIG. 6 illustrates another second tool component of a revisable implant system wherein the tool **145'** again comprises an elongate member with a distal cutting edge **144**. In one embodiment, the tool end includes a longitudinal gap **155** along a side of passageway **152** to thus allow the tool to be inserted over medial portion **110** of an implant body to then advance and cut the implant as depicted schematically in FIGS. 5A-5B. The tool end as shown in FIG. 6 can comprise a polymer member with flexible elements **158** on either side

of gap **155** to allow gap **155** to flex open when the device is being inserted over the implant. As depicted, distal cutting edge **144** may comprise a metal blade insert **160** molded into a polymer member.

FIGS. 7A-7C illustrate other embodiments of implants **200A**, **200B** and **200C** that each has a plurality of through-openings **206** in various configurations. In these embodiments, the ends are flat or planar with the openings therein. Thus, in use, there will be a plurality of tissue plugs that grow through the openings **206** to secure the implant ends in the tissue site.

FIG. 7D illustrates another embodiment of implant **200D** that has a non-planar end **201** with a plurality of through-openings **202**. In one embodiment, the ends have a plurality of elements **204** that extend in different radial angles relative to the axis **111** of the implant with each such element **204** having one or more openings therein.

FIG. 7E illustrates an implant body **200E** with ends **205A** and **205B** and medial portion **206** that comprises an axially-stretched and tensioned elastomeric material. The medial portion **206** is releasably and temporarily maintained in the axially-stretched non-repose condition by a biodissolvable portion, such as of magnesium or magnesium alloy, indicated at **208**. In this embodiment, the biodissolvable portion can comprise a tubular member with a foil-like wall or thin-wall, a plurality of thin-wall tube segments, or one or more windings or braids of biodissolvable material. The thin-wall material can be perforated as shown in FIG. 7E. The thin-wall biodissolvable material, or the biodissolvable filament of a winding or braid, can be very fine and adapted to dissolve, erode and/or absorb into the body with selected time interval ranging from about 2 weeks to 52 weeks. In another embodiment, the biodissolvable portion can be disposed in an interior portion of the implant body, in a linear or helical configuration.

Embodiments of the invention include methods for opening a collapsed or obstructed airway with devices that can be implanted into various tissues that form the airway. Embodiments of the devices include resiliently deformable materials and bioerodible materials. The deformable portion of devices, when first formed, is formed into a preferred shape which is then subsequently deformed, and stabilized in that deformed shape by incorporation or application of bioerodible materials to create a device in its implantable form. Once implanted into a tissue site, and thus exposed to an aqueous environment and subject to cellular and enzymatic action, the bioerodible portions of the device erode, thereby allowing the deformable portion of the device to return toward the preferred form. Embodiments of the method, in their simplest form, thus include implanting a device, the bioerodible portion of the device bioeroding, the device changing shape as a consequence of the bioeroding, and the tissue remodeling in accordance with the force being exerted by the shape changing of the device.

Referring again to FIG. 7E, in operation exemplary device **200E** may be implanted into an airway-interface tissue site, such as a patient's tongue. Device **200E** is configured with appropriate characteristics, such as its dimensions and flexibility, to be compatible with normal physiological function of the tissue site, such as swallowing and speech. When first implanted, biodissolvable portions **208** maintain medial portion **206** in a stretched configuration. As shown, first and second openings extend through first and second implant ends **205A** and **205B**, respectively. As the tissue adjacent the implant heals after device **200E** is implanted, these openings allow tissue plugs to grow through them, permitting each of the first and second implant ends to surround a tissue plug that

forms. This allows the ends of implant **200E** to become anchored in the tissue site before portions **208** dissolve and release the stored tension between ends **205A** and **205B**. Once biodegradable portions **208** have dissolved and pre-stretched medial portion **206** applies tension between the tissue plugs, the base of the tongue, for example, is drawn in an anterior direction to open a collapsed or obstructed airway. In some embodiments (not shown), the ends of the device may be configured to encircle the tissue plugs upon implantation, without requiring healing time for the tissue plugs to grow through the openings in the ends of the device. Further details of such devices are provided in U.S. provisional application 61/347,356, and further examples of implantation procedures are provided in U.S. application Ser. Nos. 11/969,201 and 12/937,564.

FIG. **8A** depicts the working end **210** of an elongated tool that is adapted for cutting an end portion of an implant for its removal, for example an implant of FIGS. **3A-3D**, **4**, or **7A-7D**. The tool functions similar to that of FIGS. **5A** and **6**, wherein the tool has a central bore **212** that receives the elongate medial portion of an implant body. As can be seen in FIG. **8A**, the working end **210** includes two concentric hypotubes with a notch **214** therein to push over an end portion **115** of implant **100A** of FIG. **3A**, for example. The physician can counter-rotate the hypotubes from a proximal handle end wherein blade edges **215** and **216** of the working end function as a scissors mechanism to cut the implant body. Thereafter, the implant can be easily removed from the treatment site. FIG. **8B** illustrates another working end **210'** of a similar cutting tool that has opposing notches **214** and **214'** that can receive a implant body portion and blade edges **215** and **216** can be rotated or pivoted to cut the implant.

FIG. **9** illustrates another embodiment of implant **220** that is similar to any previous embodiment except depicting a difference in surface characteristics of the implant. The end or encircling portion **225** may have smooth or slightly textured surface features and the medial portion **230** may comprise a highly lubricious surface, such as an elastomeric material having an ultra-hydrophobic surface **232** to allow for slippage of the tissue against the implant during use. Thus, a method of the invention comprises implanting a device in airway-interface tissue, securing first and second implant end portions in the tissue by permitting a tissue growth through at least one opening in an end portion, and allowing an elastomeric portion of the implant to apply retraction forces to alleviate tissue obstruction of the airway wherein an ultrahydrophobic surface of the implant prevents tissue adhesion to said surface. Ultrahydrophobic surfaces can be provided in a biocompatible polymer, as is known in the art.

In another aspect of the invention, referring to FIG. **9**, the elongate implant body is configured for implanting in an airway-interface and at least a portion of a body surface has a wetting contact angle greater than 70° , to prevent tissue adhesion and to allow tissue slippage. In other embodiments, at least a portion of a body surface has a wetting contact angle greater than 85° , or greater than 100° .

In another aspect of the invention, still referring to FIG. **9**, the elongate implant body is configured for implanting in an airway-interface and at least a portion of a body surface has an adhesive energy of less than 100 dynes/cm, less than 75 dynes/cm or less than 50 dynes/cm.

FIG. **10** illustrates another embodiment of revisable OSA implant **250** similar to previous embodiments except the medial portion **252** includes a passageway **254** configured for extending a cutting tool **255** through the passageway for cutting a distal end portion **258** of the implant. The passageway **254** can be accessed by an access opening in the oppos-

ing end (not shown) that can be identified by imaging of a marker, visual observation of a marker, by a left-in place guidewire or other suitable means or mechanism. The cutting tool **255** can comprise a scissor member, an extendable blade that is extendable from a blunt-tipped tool, any distal or proximally-facing blade, and/or any type of thermal energy emitter adapted for cutting the implant end **258**.

FIG. **11** illustrates another embodiment of revisable OSA implant **280** that has a sacrificial portion indicated at **282** that can be severed or sacrificed by an external stimulus. In one embodiment, a medial portion **283** of the implant includes electrical contacts or extending leads **284A** and **284B** that can be detachably coupled to an electrical source **285**. In FIG. **11**, the implant body comprises an elastomeric material as described above and the sacrificial portion **282** comprises a conductively doped polymer portion that acts as a fuse when subject to a very short burst of high voltage RF current. Opposing sides or aspects of the sacrificial portion **282** are coupled to electrical leads **288A** and **288B** that are embedded or molded into the implant. The use of such doped polymers for a fuse-effect for detachment of endovascular medical implants is disclosed in U.S. Pat. No. 6,458,127 to Truckai et al and issued Oct. 1, 2002, which is incorporated herein by reference. Similar doped polymers can be used in the revisable OSA implant of FIG. **11**.

FIG. **12** illustrates a method of using the OSA implant **280** of FIG. **11**, and more particularly for revising the treatment. FIG. **12** depicts that an RF current from source **285** has been delivered to melt, sever and sacrifice portion **282** of the implant thus allowing extraction of the implant from around the tissue plug.

FIGS. **13A** and **13B** illustrate another embodiment of revisable OSA implant **290** that has a sacrificial portion indicated at **282** in a medial portion of the implant that can be actuated and sacrificed by the external stimulus which then leaves the encircling portion **115** of the implant in place. The left-in-place portion of the implant can be used as an anchor for subsequent implants. In one embodiment as in FIGS. **13A-13B**, the sacrificial portion **282** can comprise an electrolytic wire that can be sacrificed over a short time interval by direct current as is known in the art. Such electrolytic wire for detachment of embolic coil implants are known in the field of aneurysm implants and treatments.

While FIGS. **11-13B** show OSA implants with two forms of sacrificial portions, it should be appreciated that similar implants can have sacrificial portions that are cut, severed or sacrificed by any external stimulus such as RF current, DC current, light energy, inductive heating etc. and may fall within the scope of the invention.

FIGS. **14** and **15** illustrate another embodiment of revisable OSA implant **300** that again includes at least one end with an encircling portion indicated at **315** that encircles or surrounds a tissue plug **316** that grows through an opening **320**. In one embodiment, the implant carries a cut wire **322** that extends in a loop with first and second wire ends **324A** and **324B** extending through one or more passageways in the implant. The cut wire **322** can be embedded in the surface of the implant surrounding the opening **320**. As can be seen in FIG. **15**, the looped cut wire **322** can be pulled proximally to cut the tissue plug **316** which then will free the implant from its attachment. In FIG. **14**, it can be seen that the cut wire ends **324A** and **324B** can have a serpentine configuration in the medial portion of the implant so as to not interfere with the tensioning and relaxation of the elastomeric medial implant portion during its use. When the cut wire is accessed and pulled relative to the implant **300**, the tissue plug **316** can be cut. It should be appreciated that other tools (not shown) may be used to sta-

bilize the implant when actuating the cut wire as in FIG. 15. The cut wire 322 can be any form of fine wire, or abrasive wire or a resistively heated wire coupled to an electrical source (not shown).

FIG. 16 depicts another revisable USA implant 300' that is similar to that of FIGS. 14-15 with the cut wire 322' configured to cut a plurality of tissue plugs 316 that have grown through openings 320 within an encircling end portion of the implant body.

FIG. 17 depicts another OSA implant 400 that is adapted for revision as previous implants and systems wherein the elongate device or implant body has first and second end portions 405A and 405B with through-openings 406A and 406B therein. The medial portion 411 of implant body 400 extends about an axis and comprises a biocompatible elastomeric material such as a silicone. In this embodiment, the medial portion comprises first and second extending portions 415A and 415B wherein one such portion can be nested in a passageway 416 of the other portion and then form proximal and distal loops or encircling end portions that define openings 406A and 406B for receiving tissue plugs therein. As can be understood from FIGS. 17 and 18A, both the extending portions 415A and 415B comprise an elastomeric material and thus combine to provide the desired retraction forces of the OSA implant.

Referring to FIGS. 18A and 18B it can be seen that if the second extending portion 415B is cut in a medial or proximal aspect of the implant, or if both the first and second extending portions 415A and 415B are cut in a proximal or medial aspect, then a proximal aspect of the first or outer extending portion 415A can be pulled in the proximal direction and the cut second extending portion 415B then will snake out of the path around the tissue plug 422. Thus, the implant can be cut in a proximal or medial aspect and can be withdrawn from the treatment site from a remote access location.

FIG. 19 depicts another OSA implant 450 that is adapted for a revision procedure and comprises an elongate implant body with first and second end portions 455A and 455B with through-openings 456A and 456B therein. This embodiment is similar to that of FIG. 17 in that medial portion 458 includes extending portions 460A and 460B comprising an elastomeric material that combine to provide the desired retraction forces of the OSA implant. The extending portions 460A and 460B are carried in a thin elastomeric sleeve 464 that has tear-away portions 465 about its ends to prevent tissue ingrowth into the passageway in the sleeve. It can be understood that by cutting the medial portion of the implant, and then pulling on an end of an extending portion 460A or 460B will cause the other free end of the implant to snake around the tissue plug similar to the method depicted in FIG. 18B. Both ends of the implant can be removed from the treatment site by this method.

The embodiments of implants shown in the figures above can be sized and shaped to conform to a treatment site in a patient's tongue, palate or other site in airway-interface tissue and to reside in an orientation and in a manner compatible with normal physiological function of the site. The overall dimensions may vary according to the full extent that human subjects vary in their anatomical dimensions, and thus the dimensions provided here are only an approximation for the purpose of illustration, and are not meant to be limiting. Any embodiment in its elongated state may typically be in the range of about 2 cm to about 10 cm in length in a releasably extended state, and the implant in a contracted state may be in the range of about 1 cm to about 6 cm in length.

Unless defined otherwise, all technical terms used herein have the same meanings as commonly understood by one of

ordinary skill in the art to which this invention belongs. Specific methods, devices, and materials are described in this application, but any methods and materials similar or equivalent to those described herein can be used in the practice of the present invention. While embodiments of the inventive device and method have been described in some detail and by way of exemplary illustrations, such illustration is for purposes of clarity of understanding only, and is not intended to be limiting.

Various terms have been used in the description to convey an understanding of the invention; it will be understood that the meaning of these various terms extends to common linguistic or grammatical variations or forms thereof. It will also be understood that when terminology referring to devices or equipment has used trade names, brand names, or common names, that these names are provided as contemporary examples, and the invention is not limited by such literal scope. Terminology that is introduced at a later date that may be reasonably understood as a derivative of a contemporary term or designating of a subset of objects embraced by a contemporary term will be understood as having been described by the now contemporary terminology.

While some theoretical considerations have been advanced in furtherance of providing an understanding of the invention the claims to the invention are not bound by such theory. Described herein are ways that embodiments of the invention may engage the anatomy and physiology of the airway, generally by opening the airway during sleep; the theoretical consideration being that by such opening of the airway, the implanted device embodiments alleviate the occurrence of apneic events. Moreover; any one or more features of any embodiment of the invention can be combined with any one or more other features of any other embodiment of the invention, without departing from the scope of the invention. Further, it should be understood that while these inventive methods and devices have been described as providing therapeutic benefit to the airway by way of intervention in tissue lining the airway, such devices and embodiments may have therapeutic application in other sites within the body, particularly luminal sites. Still further, it should be understood that the invention is not limited to the embodiments that have been set forth for purposes of exemplification, but is to be defined only by a fair reading of claims that are appended to the patent application, including the full range of equivalency to which each element thereof is entitled.

What is claimed is:

1. A method for treating an airway disorder comprising: providing an implant body having first and second end portions configured to surround first and second spaced apart tissue plugs, respectively; implanting the body in an airway-interface tissue; applying tension between the tissue plugs with the implant body to draw the tissue plugs closer together to thereby alleviate tissue obstruction of the airway; and cutting the first or second end portions to disengage the implant body from the airway-interface tissue.
2. The method of claim 1 where the implanting includes releasably maintaining the implant body in a tensioned configuration for a selected time interval.
3. The method of claim 2 wherein a portion of the implant body is releasably maintained in the tensioned configuration by a bioerodible or biodissolvable material.
4. The method of claim 3 wherein the bioerodible or biodissolvable material is carried about an exterior of the implant body.

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5. The method of claim 3 wherein the bioerodible or bio-dissolvable material is carried within an interior portion of the implant body.

6. The method of claim 1 wherein the applying tension includes releasing the implant body from a tensioned configuration to move toward a non-tensioned configuration.

7. The method of claim 6 wherein the releasing comprises allowing the bioerodible or biodissolvable material to erode or dissolve.

8. A system for revisably treating an airway disorder, comprising:

an implant body configured to conform to an airway-interface tissue site in a manner compatible with normal physiological function of the site, the implant body having a medial portion,

first and second openings extending through first and second implant ends, respectively, for permitting each of the first and second implant ends to surround a tissue plug wherein the first and second implant openings are each formed by a flexible loop at either the first or the second implant end, said flexible loops adapted to surround the tissue plugs and to disengage the implant body from the airway-interface tissue site by releasing the surrounded tissue plugs after the flexible loops have been cut, wherein at least a portion of one of the flexible loops has a higher modulus than that of the medial portion to prevent deformation of the flexible loop under tensioning forces, wherein at least one of the flexible loops comprises a proximal portion of a lower modulus material similar to a modulus of the medial portion of the implant body, and a terminal part having a higher modulus to prevent its deformation under tensioning forces.

9. The method of claim 1, wherein the first and second end portions of the implant body each comprise a loop, and wherein at least a portion of one of the loops has a higher modulus than that of a medial portion of the implant body to prevent deformation of the loop under tensioning forces.

10. The method of claim 1 where the first and second tissue plugs grow through the first and second end portions of the implant body, respectively, after the body is implanted.

11. The method of claim 1 where the first and second end portions are provided in the implant body in a releasably tensioned configuration, the releasably tensioned configuration being releasably maintained by a bioerodible or biodissolvable material carried by a medial portion of the implant body.

12. The method of claim 1 further including cutting said tissue plugs and extracting the implant from the tissue to revise treating.

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13. The method of claim 1 further including extracting the implant body from the airway-interface tissue to revise treating.

14. A system for revisably treating an airway disorder, comprising:

an implant body configured to conform to an airway-interface tissue site in a manner compatible with normal physiological function of the site, the implant body having a medial portion,

first and second openings extending through first and second implant ends, respectively, for permitting each of the first and second implant ends to surround a tissue plug wherein the first and second implant openings are each formed by a flexible loop at either the first or the second implant end, said flexible loops adapted to surround the tissue plugs and to disengage the implant body from the airway-interface tissue site by releasing the surrounded tissue plugs after the flexible loops have been cut, wherein at least a portion of one of the flexible loops has a higher modulus than that of the medial portion to prevent deformation of the flexible loop under tensioning forces.

15. The system of claim 14 further comprising a cutting element configured for removal of the implant body from the site.

16. The system of claim 15 wherein the cutting element comprises at least one of a pivotable blade edge, a rotatable sleeve with a blade edge, an axially translatable blade edge, and a cut wire.

17. The system of claim 14 wherein the medial portion is configured for implantation in the airway-interface tissue site in a non-repose condition.

18. The system of claim 17 wherein the medial portion is configured to be releasably maintained in the non-repose condition by a bioerodible or biodissolvable material carried by said medial portion.

19. The system of claim 14 wherein the first and second openings of the first and second implant ends are configured to allow the tissue plugs to grow therethrough after the implant body has been implanted in the airway-interface tissue site.

20. The system of claim 14 wherein the medial portion comprises an elastomeric material.

21. The system of claim 14, wherein the loops comprise an elastomeric material.

22. The method of claim 9, wherein the least one of the loops comprise a proximal portion of a lower modulus material similar to a modulus of the medial portion of the implant body, and a terminal part having a higher modulus to prevent its deformation under tensioning forces.

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